

(12) INTERNATIONAL APPLICATION PUBLISHED UNDER THE PATENT COOPERATION TREATY (PCT)

(19) World Intellectual Property Organization  
International Bureau



(43) International Publication Date  
15 March 2001 (15.03.2001)

PCT

(10) International Publication Number  
**WO 01/17567 A2**

(51) International Patent Classification<sup>7</sup>: **A61K 49/00**

(21) International Application Number: **PCT/GB00/03373**

(22) International Filing Date:  
1 September 2000 (01.09.2000)

(25) Filing Language: **English**

(26) Publication Language: **English**

(30) Priority Data:  
9920758.1 3 September 1999 (03.09.1999) GB

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(81) Designated States (national): AE, AG, AL, AM, AT, AU, AZ, BA, BB, BG, BR, BY, BZ, CA, CH, CN, CR, CU, CZ, DE, DK, DM, DZ, EE, ES, FI, GB, GD, GE, GH, GM, HR, HU, ID, IL, IN, IS, JP, KE, KG, KP, KR, KZ, LC, LK, LR, LS, LT, LU, LV, MA, MD, MG, MK, MN, MW, MX, MZ, NO, NZ, PL, PT, RO, RU, SD, SE, SG, SI, SK, SL, TJ, TM, TR, TT, TZ, UA, UG, US, UZ, VN, YU, ZA, ZW.

(84) Designated States (regional): ARIPO patent (GH, GM, KE, LS, MW, MZ, SD, SL, SZ, TZ, UG, ZW), Eurasian patent (AM, AZ, BY, KG, KZ, MD, RU, TJ, TM), European patent (AT, BE, CH, CY, DE, DK, ES, FI, FR, GB, GR, IE, IT, LU, MC, NL, PT, SE), OAPI patent (BF, BJ, CF, CG, CI, CM, GA, GN, GW, ML, MR, NE, SN, TD, TG).

**Published:**

— *Without international search report and to be republished upon receipt of that report.*

*For two-letter codes and other abbreviations, refer to the "Guidance Notes on Codes and Abbreviations" appearing at the beginning of each regular issue of the PCT Gazette.*



**WO 01/17567 A2**

(54) Title: **IMPROVED CONTAINER COMPOSITION FOR DIAGNOSTIC AGENTS**

(57) Abstract: The present invention relates to improved containers for diagnostic agents, which are metal complex contrast agents for MRI or X-ray imaging, or hyperpolarised materials where the container has an internal coating of SiO<sub>2</sub>. The silica coating is preferably deposited by a plasma chemical vapour deposition (PCVD) process.

Improved Container Composition for Diagnostic AgentsSummary of the Invention

5 The present invention relates to improved containers for diagnostic agents, which are metal complex contrast agents for MRI or X-ray imaging, or hyperpolarised materials, where the container has an internal coating of silica (ie. silicon dioxide or  $\text{SiO}_2$ ). The silica coating is preferably deposited by a plasma chemical vapour deposition (PCVD) process.

10 Field of the Invention

The present invention relates to diagnostic agents, especially for *in vivo* use, in a coated container, where the container has an internal coating of silica coating on the surface(s) which are in contact with the diagnostic agent.

15 Background to the Invention

US 4385086 (1983) discloses that a variety of materials (eg. soda glass, ceramics and metals) can be coated with highly oxidised silicon to prevent the leaching of metal ions from the material.

20 FR 2697014 A1 (1994) discloses the silica coating of the bottles, flasks, ampoules etc. for use with food or liquid pharmaceutical products to reduce leaching of metals into the liquid contents of the container.

25 DE 29609958 U1 discloses that glass containers having an internal coating of  $\text{SiO}_2$  prepared by PCVD are useful for the storage of pharmaceutical or diagnostic solutions.

JP 11-99192A discloses that silica-coated vials (prepared by a chemical coating and pyrolysis method), are useful to prevent adsorption of radiopharmaceutical products such as  $^{201}\text{Tl}$  solution to the surface of the glass. The silica coating of these vials is manufactured by the method described in JP 2815595 B which involves treating the glass 5 surface with a silyl tetraisocyanate vapour in a carrier gas, followed by heating at high temperatures. JP 2815595 B also discloses that such a silica coating is useful to prevent leaching of impurities such as alkali from the glass into medical products.

US 5612103 discloses the use of coatings of deuterated polymers to inhibit the 10 depolarisation of hyperpolarised gases within a container. WO 99/08941 discloses the use of glass vessels coated with a sol-gel, preferably an aluminosilicate glass, for the same purpose. WO 99/17304 discloses the use of a container made of a special glass having a low iron content for the same purpose.

15 Summary of the Invention

The present invention relates to silica-coated containers in combination with the following categories of diagnostic agents:

- (i) lyophilised kits or liquid or solution formulations for the preparation of 20 MRI contrast agents which comprise metal complexes of paramagnetic metal ions;
- (ii) lyophilised kits or liquid or solution formulations of X-ray contrast agents which comprise metal complexes of radiopaque metal ions;
- (iii) hyperpolarised gases such as  $^{129}\text{Xe}$  or  $^3\text{He}$  or other hyperpolarised materials.

Detailed Description of the Invention

The present invention relates to a composition comprising a diagnostic agent in a container which has a silica coating on the inner surface. Suitable such containers are 5 commercially available, e.g. a silica-coated vial called Silicoat is available from Fuji Glass KK, and a silica-coated vial called Type I Plus is available from Schott Glas. The Type I Plus vial is prepared by a plasma chemical vapour deposition (PCVD) process.

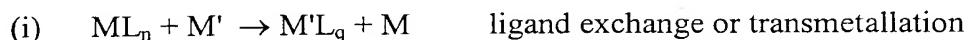
Other containers can be coated with silica using known methods, where the silicon-10 containing layer is deposited from either gas phase or liquid phase contact with the container surface(s), with optional pyrolysis and/or oxidation to convert the deposited silicon-containing layer to  $\text{SiO}_2$ . Such methods are known in the art. Using either approach, irregularly-shaped containers can be coated. Examples of gas phase deposition are PCVD, and the process of JP 2815595 B which uses silyl tetraisocyanate vapour in 15 carrier gas. The latter process delivers the silicon-containing layer in a single step, with pyrolysis of silyl tetraisocyanate required to give the final product, i.e. the coated vial. Depending on the efficiency of the heat transfer, the coating layer may not be pure  $\text{SiO}_2$ , 20 but perhaps contain carbon or nitrogen. The silica-coated vial prepared by PCVD has advantages over the disclosures of JP 2815595 B and JP 11-99192A, because the  $\text{SiO}_2$  layer prepared by PCVD is in fact developed by multiple exposure to the vapour phase silicon reagent. The result is a much more uniform layer of high purity  $\text{SiO}_2$ , which is mechanically sound and resistant to abrasion etc. Hence PCVD is a preferred process for use in containers of the present invention.

The term “diagnostic agent” as used herein means either a hyperpolarised material or a non-radioactive metal complex which is an MRI contrast agent or an X-ray contrast agent. The “hyperpolarised material” can be a hyperpolarised gas, such as  $^{129}\text{Xe}$  or  $^3\text{He}$ , or a  $^{13}\text{C}$ - or  $^{15}\text{N}$ -enriched labelled molecule or a  $^{19}\text{F}$ - or  $^{31}\text{P}$ - containing molecule where the 5 MRI active nucleus of interest has been hyperpolarised by a polarisation transfer process. The silica coatings of the present invention are believed to be especially useful for hyperpolarised  $^{129}\text{Xe}$  compositions, since xenon has low solubility in silica. The diagnostic agent may be used for *in vivo* and/or *in vitro* diagnosis. The metal complex contrast agents of the present invention are preferably for *in vivo* use.

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The term “metal complex” as used herein means a coordination complex of a metal (M) with an organic ligand (L). This is to be contrasted with an uncomplexed or free metal ion e.g. the monovalent thallium cation  $\text{Tl}^+$ . The term ‘organic ligand’ as used herein means a carbon-containing compound which comprises at least one heteroatom suitable for 15 coordination to a metal, such as N, O, S, P or Se, or combinations thereof. Examples of organic ligands are amines, hydrazines, ethers such as crown ethers, thiols or thioethers, oximes, phosphines, amides, pyridines or other heterocyclic molecules such as quinolines, aminocarboxylate ligands such as DTPA, DOTA or HEDTA. The metal donor atoms can be arranged together to form chelating agents or polydentate ligands such as 20 diaminedioximes, hydroxyquinolines, diaminedithiols, diamidedithiols; or macrocyclic ligands such as DOTA, and many more combinations as is well known in the art. MRI contrast agents are typically metal complexes, where the metal is a paramagnetic metal ion such as gadolinium (III) of aminocarboxylate ligands such as DTPA or DOTA. X-ray contrast agents can also be metal complexes, where the metal is radiopaque, such as 25 bismuth or tungsten.

When the diagnostic agent is or comprises a metal complex, if leached metal ions (M') such as aluminium or sodium, are leached from glass into the product, these leached metal ions may adversely affect the product in a manner which goes beyond the simple 5 presence of M' as an impurity:



10 where:

M is the metal of the desired metal complex product,

L is the organic ligand;

M' is the leached metal ion;

ML<sub>n</sub> is the metal complex product, which may comprise 2 or more different 15 organic ligands L;

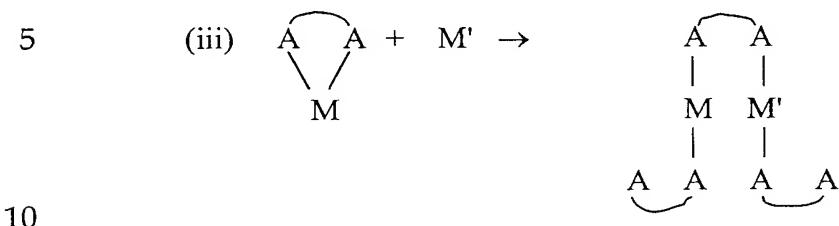
n is number of ligands (L) attached to M and is an integer of value 1 to 8;

M'L<sub>q</sub> is the metal complex impurity;

q is number of ligands (L) attached to M' and is an integer of value 1 to 8.

20 Process (i) can occur when the leached metal or metals (M') have greater affinity for one or more of the organic ligands (L) than the metal (M) of the contrast agent product. In addition to, or instead of equation (i), complexation (ii) may also occur. This leads to the presence of undesirable M'L<sub>q</sub> impurities in the product ML<sub>n</sub>.

When L is a multidentate ligand, such as a chelating agent the number of metal donor sites (A) per ligand (L) may be 2, 3, 4, 5, 6 or 8 typically. In that case, a process which is a special case of equation (i) above could occur as follows:



note: the curved lines represent the chain of atoms linking the A groups.

leading to dimeric or oligomeric binuclear or polynuclear metal complexes  
 15 involving both M and M'. The leached metal (M') may be less amenable to chelation by polydentate ligand (L), and hence favour such polynuclear species, even when M does not. This could result when the energetics are less favourable, e.g. M' is too small for two A groups to coordinate without undue steric interactions. In this way, a single M' atom could potentially generate a polynuclear or oligomeric species which comprises several M atoms.  
 20 Clearly, the greater the denticity of the ligand L (i.e. the greater the number of A metal donor sites), the greater the potential complexity of the product.

The presence of such species may present impurity or manufacturing or irreproducibility problems due to vial-to-vial variations, or toxicity problems due to the  
 25 impurity species or particulate problems when insoluble materials result, eg. when  $M'L_q$  is highly insoluble. Such insoluble impurities may also potentially serve to promote co-precipitation of the desired product  $ML_n$ . Particulate problems would be a serious safety problem for products intended for human injection. Impurity species may also adversely

affect product imaging performance by e.g. localising in undesirable background areas *in vivo* which adversely impact the image to be made.

In the light of the above, it can be seen that the influence of leachable metal ions (M'), can have effects which go far beyond simply the presence of metal ion impurities alone in solution. This is important for metal complex contrast agent products, and is not recognised by JP 11-99192A which makes no specific reference to metal complexes. The  $^{201}\text{Tl}$  radioisotope taught by JP 11-99192 A is an uncomplexed radiometal in the chemical form of the Tl(I) cation  $\text{Tl}^+$ . The teaching of JP 11-99192 A relates only to adsorption effects *via* an ion exchange mechanism for the  $^{201}\text{Tl}$  cation  $\text{Tl}^+$  with the non-radioactive  $\text{Na}^+$  and  $\text{K}^+$  ions of the glass container walls. The main thrust of JP 11-99192 A is to a radiopharmaceutical vial having reversed text characters on the surface of the container.

For uncoated glass containers, the leaching of metal ions from the glass can potentially be overcome by washing with dilute aqueous acid solutions (to remove relatively labile leachable metal ions), following by rinsing and (optionally) drying steps, before the container is loaded with product. The layer of  $\text{SiO}_2$  suppresses any such leaching of metal ions (M'), and hence obviates the need for any such washing steps. This is particularly important for diagnostic products intended for human use, especially for human injection, since these washing steps must be done in a sterile manner, hence although such steps may be straightforward, their removal represents a significant improvement.

Hyperpolarised materials are non-radioactive materials which have a finite lifetime due to the decay process from the hyperpolarised state to the ground state, i.e.

depolarisation. The rate of depolarisation is believed to be increased in the presence of paramagnetic species, especially molecular oxygen, or paramagnetic metal ions e.g.  $\text{Fe}^{3+}$ . The composition of the present invention where the diagnostic agent is a hyperpolarised material, therefore provides improved containers where an inert layer of essentially pure 5  $\text{SiO}_2$  is interposed between the hyperpolarised material and the normal walls of the container.

The  $\text{SiO}_2$  layer is free from any metallic ions or paramagnetic species and is of high chemical purity, especially when it is deposited by CPVD. It is hence expected to 10 represent an improvement over prior art approaches to increasing the lifetime of hyperpolarised species.

Silica coating techniques based on gas phase deposition, eg. PCVD, can be adapted to coat the inner surfaces of containers or vessels of almost any shape or size. Hence it is 15 anticipated that the container compositions of the present invention can be applied to production apparatus as well as storage and transport vessels. The silica coating can also readily be applied to non-rigid, flexible materials such as thin plastics. Such containers could be used e.g. for containing doses of hyperpolarised gases such as  $^{129}\text{Xe}$  or  $^3\text{He}$  in plastic bags with an inner silica coating, as unit doses for human administration by 20 inhalation.

Example 1 shows that a silica-coated vial (the Type 1 Plus vial) does prevent the leaching of silicon, sodium, aluminium and boron ions from the glass, even under stress conditions.

ExperimentalExample 1

5 Groups of 10 Type I Plus vials (Schott Glas) were subjected to a series of stress tests to demonstrate the robustness of the silica coating with respect to leachable ions. The basic test was the resistance of the coating to the leaching of cations when autoclaved with 0.04M aqueous HCl. This test was performed after vials were exposed to the following stress conditions:

10

1. vials were washed, and then pyrogen baked. 2ml of 0.04M HCl was added and the vials sealed. Test vials were autoclaved, then stored upright at 40°C before testing for leachable cations.
2. vials were stored for 6 weeks at -196°C, then washed and pyrogen baked. 2ml of 0.04M HCl was added to each vial, and the vials were then sealed, autoclaved and tested for leachable cations.
- 15 3. as for test 2, except that the vials were stored at -70°C, -20°C, +20°C and +40°C/75% relative humidity.
4. further tests included: vials pyrogen baked 3 times; vials containing 0.04M HCl 20 autoclaved three times; vials gamma irradiated (35.4 – 36.2 kGy dose).

25 All test solutions were measured by ICP for silicon, sodium, aluminium and boron, those cations considered to be most leachable from the vial surface. The results are given in Table 1.

25

Table 1

Test Number	Si	Na	Al	B
1	0.149	Nd	0.006	Nd
2	0.163	Nd	Nd	Nd
3	0.167	Nd	Nd	Nd
	-70°C			
	-20°C	0.005	0.002	0.002
	+20°C	0.009	0.005	0.003
	+40°C	0.006	0.002	0.002
4	0.110	Nd	0.010	Nd
	bake			
	X3	0.012	Nd	0.006
	Gamma	0.003	Nd	Nd

5 Note: each table entry is the mean of 12 batch runs, each batch of 10 vials (i.e. 120 vials tested), expressed in  $\mu\text{g}/\text{cm}^3$  of test solution.

Nd = not detected. Detection limits (in  $\mu\text{g}/\text{cm}^3$ ): B - 0.004  
Si - 0.003  
Na - 0.004  
Al - 0.004

Claims

5        1. A composition which comprises a diagnostic agent in a container which has a silica coating on the inner surface, characterised in that the diagnostic agent comprises a non-radioactive metal complex or a hyperpolarised material.

10      2. The composition of claim 1 where the diagnostic agent comprises a non-radioactive metal complex.

15      3. The composition of claim 2 where the metal complex is an MRI contrast agent.

4. The composition of claim 2 where the metal complex is an X-ray contrast agent

15      5. The composition of claim 1 where the diagnostic agent comprises a hyperpolarised material.

20      6. The composition of claim 5 where the hyperpolarised material comprises hyperpolarised  $^{129}\text{Xe}$  or  $^3\text{He}$  gas.

25      7. The composition of claim 5 where the hyperpolarised material comprises one or more hyperpolarised  $^{13}\text{C}$  atoms.

25      8. The composition of claims 1 to 7 where the silica coating is deposited by PCVD.

9. The composition of claims 1 to 8 where the silica coating comprises pure SiO<sub>2</sub>.

(19) World Intellectual Property Organization  
International Bureau(43) International Publication Date  
15 March 2001 (15.03.2001)

PCT

(10) International Publication Number  
WO 01/17567 A3(51) International Patent Classification<sup>7</sup>: A61K 49/00,  
49/04(74) Agents: CANNING, Lewis, Reuben et al.; Nycomed  
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Road, Amersham, Buckinghamshire HP7 9LL (GB).

(21) International Application Number: PCT/GB00/03373

(81) Designated States (national): AE, AG, AL, AM, AT, AU,  
AZ, BA, BB, BG, BR, BY, BZ, CA, CH, CN, CR, CU, CZ,  
DE, DK, DM, DZ, EE, ES, FI, GB, GD, GE, GH, GM, HR,  
HU, ID, IL, IN, IS, JP, KE, KG, KP, KR, KZ, LC, LK, LR,  
LS, LT, LU, LV, MA, MD, MG, MK, MN, MW, MX, MZ,  
NO, NZ, PL, PT, RO, RU, SD, SE, SG, SI, SK, SL, TJ, TM,  
TR, TT, TZ, UA, UG, US, UZ, VN, YU, ZA, ZW.(22) International Filing Date:  
1 September 2000 (01.09.2000)(84) Designated States (regional): ARIPO patent (GH, GM,  
KE, LS, MW, MZ, SD, SL, SZ, TZ, UG, ZW), Eurasian  
patent (AM, AZ, BY, KG, KZ, MD, RU, TJ, TM), European  
patent (AT, BE, CH, CY, DE, DK, ES, FI, FR, GB, GR, IE,  
IT, LU, MC, NL, PT, SE), OAPI patent (BF, BJ, CF, CG,  
CI, CM, GA, GN, GW, ML, MR, NE, SN, TD, TG).

(25) Filing Language: English

**Published:**

— with international search report

(26) Publication Language: English

(88) Date of publication of the international search report:  
15 November 2001(30) Priority Data:  
9920758.1 3 September 1999 (03.09.1999) GBFor two-letter codes and other abbreviations, refer to the "Guid-  
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HP7 9LL (GB). CANNING, Lewis, Reuben [GB/GB];  
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WO 01/17567 A3

(54) Title: IMPROVED CONTAINER COMPOSITION FOR DIAGNOSTIC AGENTS

(57) Abstract: The present invention relates to improved containers for diagnostic agents, which are metal complex contrast agents for MRI or X-ray imaging, or hyperpolarised materials where the container has an internal coating of SiO<sub>2</sub>. The silica coating is preferably deposited by a plasma chemical vapour deposition (PCVD) process.

# INTERNATIONAL SEARCH REPORT

Inte. .onal Application No

PCT/GB 00/03373

**A. CLASSIFICATION OF SUBJECT MATTER**  
 IPC 7 A61K49/00 A61K49/04

According to International Patent Classification (IPC) or to both national classification and IPC

**B. FIELDS SEARCHED**

Minimum documentation searched (classification system followed by classification symbols)  
 IPC 7 A61K C03C C23C

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

Electronic data base consulted during the international search (name of data base and, where practical, search terms used)

EPO-Internal, WPI Data, PAJ, EMBASE, BIOSIS, CHEM ABS Data, MEDLINE

**C. DOCUMENTS CONSIDERED TO BE RELEVANT**

Category °	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X	US 5 565 248 A (PLESTER GEORGE ET AL) 15 October 1996 (1996-10-15) abstract column 2, line 25-35 column 5, line 25-40 ---	1,2,4-6, 9-11,14
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Patent family members are listed in annex.

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Date of the actual completion of the international search  20 June 2001	Date of mailing of the international search report  27/06/2001
Name and mailing address of the ISA European Patent Office, P.B. 5818 Patentlaan 2 NL - 2280 HV Rijswijk Tel. (+31-70) 340-2040, Tx. 31 651 epo nl, Fax: (+31-70) 340-3016	Authorized officer  Gonzalez Ramon, N

# INTERNATIONAL SEARCH REPORT

## Information on patent family members

International Application No

PCT/GB 00/03373

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